



# Cost-Benefit Analysis of 3D FE Modeling of the Tibia Throughout the Stance Phase

## Background

### Bone Stress Injuries (BSIs)

- Can be caused by repetitive forces from running [1]
- 40-60% of BSIs occur in the tibia [2]

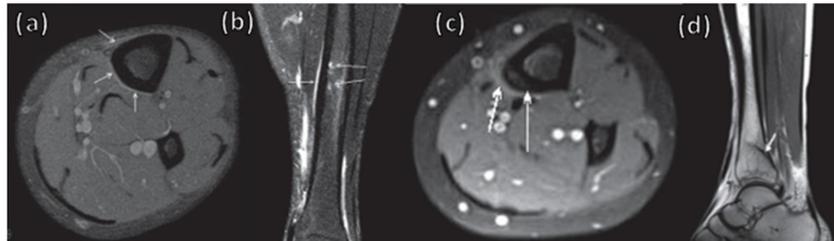
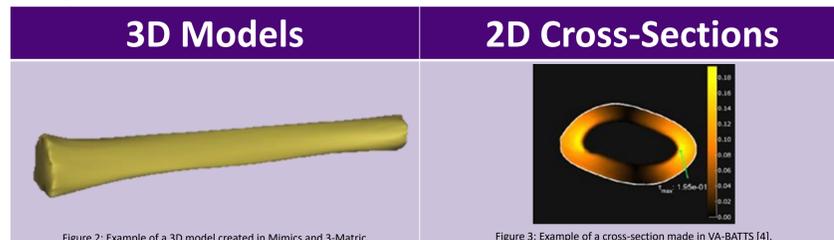


Figure 1: MRIs of BSIs with increased grading scales defined by Gmachowska et al. [3]. (a) Grade 1 with periosteal edema (b) Grade 2 with bone marrow and periosteal edema (c) Grade 3 with cortical abnormalities, bone marrow and periosteal edema (d) Grade 4 with a fracture line. Images adapted from [3].

### Computational Models

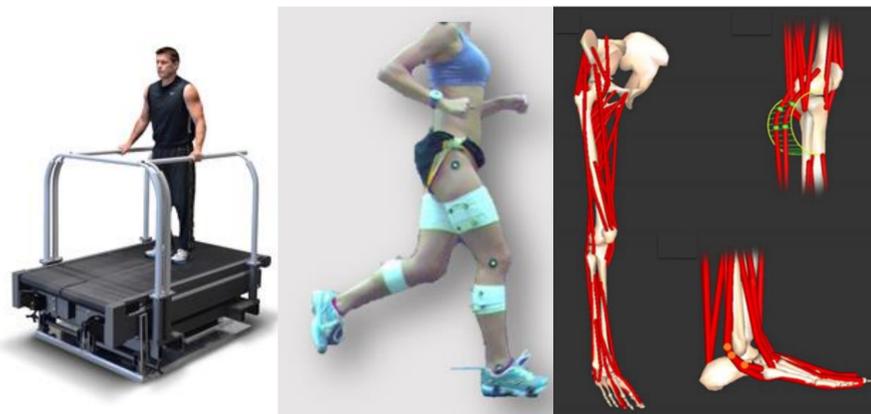


### Objectives:

1. Find the differences between the FEA results in 3D models and 2D cross-sectional models
2. Identify if these differences are clinically significant
3. Determine limitations in each method

## Data Collection

### Collection of Kinetic/Kinematic Data



- Finally, static optimization and vector summation was performed with the distal tibia reaction forces and muscle forces to estimate the forces affecting the distal tibia

### MR Image Acquisition

- MR images were collected of the frontal, coronal, and sagittal plane of the subject's right tibias with a 1.5-T scanner with a torso coil
- Vitamin E capsules were used to assist with aligning the coordinate system

## FEA on 3D Models

### Creating and Meshing 3D Models

#### Generating Models (in Mimics and 3-Matic):

- Semiautomatic segmentation
- Wrapped and smoothed
- Inner bone subtracted from entire bone

#### Orientation (in Mimics and 3-Matic):

- Defined centroids used to determine current/desired orientations
- Rotated/translated model as needed

#### Trimming (in 3-Matic):

- Trimmed models at the distal 15% and proximal 85%

### Performing FEA in ANSYS Mechanical:

#### Material properties:

- Young's modulus: 17.19 GPa | Poisson's ratio : 0.3 [8]
- Ran FEA at each 10% of the stance phase

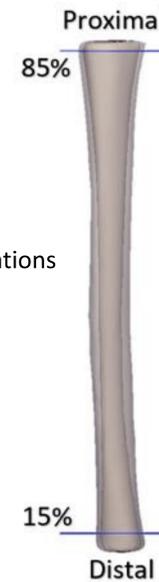


Figure 7: Representation of trimming 3D models.

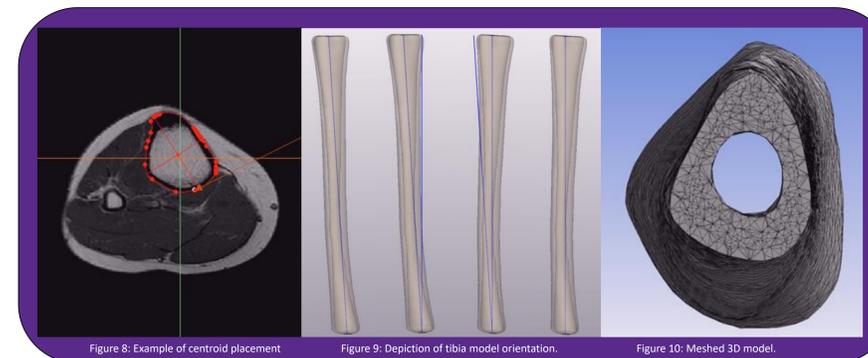


Figure 8: Example of centroid placement

Figure 9: Depiction of tibia model orientation.

Figure 10: Meshed 3D model.

## FEA on 2D Cross-Sections

### Using VA-BATTS [4]

#### Adapting for MR images:

- Uniform Young's Modulus
- Polygon Fit
- Inverted and Rotated Image

#### Solving for Strains:

- Young's Modulus: 17.19 GPa [8]
- Hooke's Law:

$$\epsilon = \frac{\sigma}{E}$$

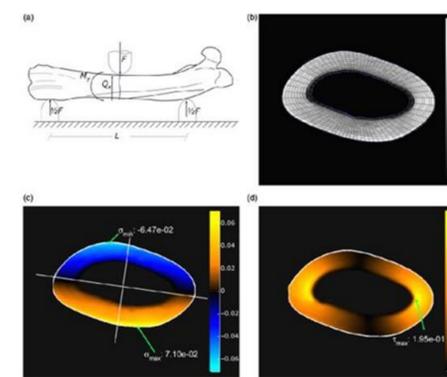


Figure 11: An example of a 2D cross-section made in VA-BATTS [4].

## Results/Discussion

### Results

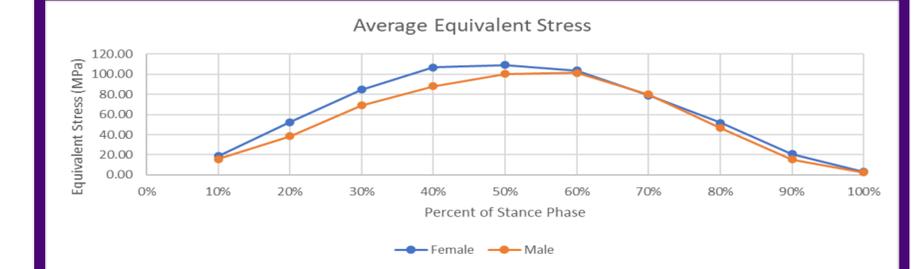


Figure 12: Average maximum Von Mises stress across the stance phase.

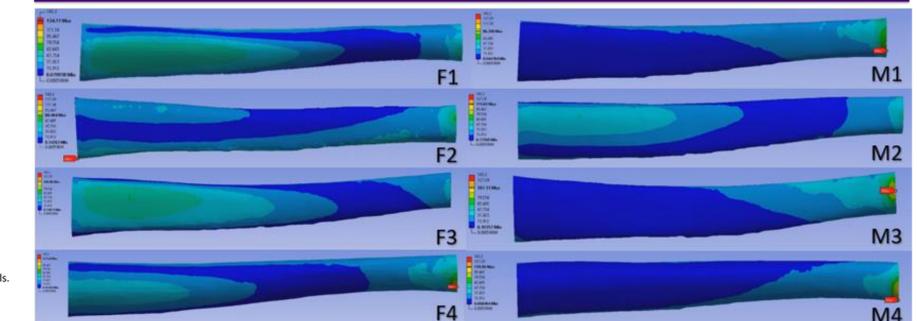


Figure 13: Maximum Von Mises stress distribution for all participants.

Metric	All	Males	Females	Published Values
Max Von Mises Stress (MPa)	104.76 ± 16.59	101.21 ± 9.35	109.33 ± 19.34	102.1 (Male) 120.24 (Female) [9]
Max Von Mises Strain (µε)	6100.31 ± 965.33	5897.58 ± 542.31	6361.60 ± 1123.37	7939.79 ± 1588.74 [8]
Max Normal Strain (µε)	3684.91 ± 1284.91	4085.38 ± 1260.31	3284.45 ± 1180.19	Max Compressive Strains: 2800-4800 [10]

### Discussion

- Average maximum equivalent stress/strain occurred towards the middle of the stance phase
- Variances between collected values and published values could be due to differences in methodology or subject populations such as:
  - [9] included trabecular and cortical bone and only used a male and a female
  - [8] did not use subject specific models
  - [10] only used male models
- Study Limitations: small population size, cortical bone-only hollow models, and a generalized Young's modulus
- Next Steps: Analyze 2D cross-sectional data and perform data analysis

## References

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